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Surface profiling apparatus

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SURFACE PROFILING APPARATUS

Field of the Invention

The invention relates to surface profiling apparatus and to respiratory function
5 monitoring apparatus incorporating the surface profiling apparatus.

Background to the Invention

There are many situations in which there is a requirement to measure or
monitor the shape or profile of a surface. An important example is the monitoring of
10 respiratory function through non-invasive measurement of thoracoabdominal surface
movement. Current approaches to carrying out volumetric measurement of respiratory
function include inductance plethysmography in which a continuous, low-voltage
electrical signal is passed through two coils of wire placed around a subject's rib cage
and abdomen respectively. In this approach the changes in chest and abdomen
15 volumes are taken to be equivalent to the changes in metric of the chest and
abdomen compartments respectively. However, accurate calibration of this type of
device is difficult and it gives a limited picture of the movements involved. Alternative
approaches using cameras to record the movement of markers or grids of light on the
chest have also been employed, but these are extremely complex techniques and
20 they do not allow free ambulatory movement of the subject.

Various fibre-optic based devices have been developed which measure
respiration according to the two degree of freedom system associated with inductance
plethysmography. These devices perform measurements of the perimeter of the chest
and abdomen, or depth of breathing, using optical fibre and fibre Bragg gratings as
25 strain or displacement transducers. This technique ignores distortions which occur in
the rib cage with increasing volumes of ventilation and relies on additional parameters
which compensate for geometrical factors, cumulatively lumping them as part of
coefficients in most cases as part of a calibration procedure.

Whilst these methods can typically provide accurate results ($\pm 5\%$ error in tidal
30 volume) for a single set of stationary quiet breathing conditions, accuracy is degraded
with changes in posture as well as breathing pattern and magnitude. In validation
studies of devices using these techniques, errors of as much as $\pm 30\%$ in respired tidal
volume were not uncommon in a significant number of samples (up to 20% of the
sample population). Such devices must also be re-calibrated frequently if the results

produced are to be regarded as more than qualitative. As such they generally find application as monitors for recumbent patients, for example monitoring of sleep and postoperative apnoeas.

5 **Summary of the Invention**

According to a first aspect of the invention there is provided surface profiling apparatus comprising:

an optical waveguide including a plurality of sensor sections in which a plurality of optical waveguide grating curvature sensing devices are respectively provided; and
10 optical interrogation means operable to interrogate the optical waveguide grating curvature sensing devices, to determine the curvature experienced by each device,

whereby a profile of a surface to which the sensor sections of the optical waveguide are coupled may be constructed from the curvatures sensed by the optical
15 waveguide grating curvature sensing devices.

The optical waveguide is preferably an optical fibre, which may be a silica-glass optical fibre or a polymer optical fibre.

The surface may be an exterior surface or may be an internal surface within a structure.

20 The optical fibre preferably comprises a core, an inner cladding layer surrounding the core, and at least a first outer cladding layer surrounding the inner cladding layer, the refractive index of the inner cladding layer being less than the refractive index of the core, and the refractive index of the first outer cladding layer being less than the refractive index of the inner cladding layer.

25 Desirably, the first outer cladding layer is thick enough to isolate light propagating within a cladding mode of the inner cladding layer from a medium surrounding the first outer cladding layer. The optical fibre may be progressive three layered optical fibre or matched index optical fibre.

30 The optical fibre may further comprise a second outer cladding layer surrounding the first outer cladding layer in order to isolate light propagating within a cladding mode of the inner cladding layer from a medium surrounding the outermost cladding layer, the refractive index of the second outer cladding layer being less than the refractive index of the first outer cladding layer. The optical fibre may comprise a plurality of outer cladding layers, each outer cladding layer surrounding a preceding

outer cladding layer and having a lower refractive index than the preceding outer cladding layer.

The refractive index profile of the fibre core may be radially asymmetric. Alternatively or additionally the refractive index profile of one or more cladding layers of the fibre may be radially asymmetric.

A plurality of optical waveguides including a plurality of sensor sections may be provided.

The optical waveguide grating curvature sensing devices preferably comprise optical waveguide grating devices. An optical waveguide grating device may comprise a long period grating. The long period grating may be radially asymmetric. The long period grating may include one or more phase-shifts within its periodic refractive index variation. Alternatively or additionally the period of the refractive index variation of one or more parts of the long period grating may be chirped.

An optical waveguide grating device may alternatively comprise two long period gratings arranged to together define an in-line Mach-Zehnder interferometer. An optical waveguide grating device may further alternatively comprise an optical waveguide Bragg grating, or two optical waveguide Bragg gratings arranged to together define a Fabry-Perot etalon.

The surface profiling apparatus may further comprise coupling means for coupling the sensor sections of the optical waveguide to the surface to be profiled. The coupling means preferably comprises a carrier member, the sensor sections of the optical waveguide being fixed to or embedded within the carrier member. The coupling means may alternatively comprise a plurality of carrier members mounted on a support structure, one or more optical waveguide sensor sections being fixed to or embedded within each carrier member. The or each carrier member is preferably deformable and most preferably comprises a flexible skin fixed to a partially rigid, expandable skeleton structure. The carrier member or support structure is preferably of a corresponding size and shape to the surface to be profiled, such that a close fit is provided between the or each carrier member and the surface.

The optical interrogation means is preferably a derivative spectroscopy or synthetic heterodyne based optical interrogation means operable to detect changes in the spectral profile of an optical waveguide grating device. The optical interrogation means preferably comprises an optical source operable to generate a wavelength modulated optical signal at a wavelength within the spectral range of an optical

waveguide grating device to be interrogated, the optical source being optically coupled to an one, input, end of the respective optical waveguide, and optical detection means optically coupled to the other, output, end of the optical waveguide and being operable to detect changes in the spectral transmission profile of the optical waveguide grating device being interrogated and to thereby determine the curvature experienced by the grating device. The optical signal preferably has a narrow spectral bandwidth compared with the spectral bandwidth of the optical waveguide grating device to be interrogated.

The optical source may comprise a plurality of wavelength modulated lasers, the wavelength of each laser output optical signal lying within the spectral range of its respective optical waveguide grating device. One or each of the wavelength modulated lasers may be distributed feedback lasers, the injection current provided to the laser from its drive unit being modulated at a desired frequency to thereby produce a wavelength modulation on the optical output signal generated by the laser. One or each of the wavelength modulated lasers may alternatively comprise fibre lasers having a fibre Bragg grating for one or both of the laser mirrors, the or each fibre Bragg grating being coupled to tuning means operable to vary the resonant wavelength of the or each fibre Bragg grating at a desired modulation frequency, thereby apply a corresponding wavelength modulation to the laser output signal.

The optical source may alternatively or additionally comprise a plurality of fibre Bragg gratings, each grating having a different resonant wavelength lying within the spectral profile of a respective optical waveguide grating device, and being coupled to tuning means operable to vary its resonant wavelength at a desired modulation frequency, and a broad bandwidth optical source for illuminating the gratings, the light reflected by each grating thereby forming a wavelength modulated narrow bandwidth optical signal. The broad bandwidth optical source may be a superluminescent light emitting diode or an edge-emitting light emitting diode.

Preferably, a different modulation frequency is used for each optical waveguide grating device provided in a single optical waveguide.

The optical source may further alternatively comprise a wavelength tunable optical source, operable to generate a narrow bandwidth optical signal, and wavelength modulation apparatus operable to apply a wavelength modulation at a desired modulation frequency to the generated optical signal. The wavelength tunable

optical source may be a distributed feedback laser or a Fabry-Perot etalon based laser.

5 The optical detection means preferably comprises a photodetector optically coupled to the output end of the or each optical waveguide and a plurality, corresponding to the number of optical waveguide grating devices provided within the
10 respective waveguide, of lock-in amplifiers or synchronous detectors each operable to measure the amplitude of a detected optical signal at the modulation frequency associated with a particular optical waveguide grating device and a harmonic of the modulation frequency, most preferably the second harmonic. The optical detection
15 means preferably further comprises data processing means connected to the or each photodetector, operable to calculate the ratio of the amplitudes. The data processing means is desirably further operable to calculate the arc tangent of the ratio of the amplitudes, to which the curvature experienced by the optical waveguide grating device under interrogation is linearly related. The data processing means is preferably
20 further operable to generate a two-dimensional or three-dimensional wire-frame profile of the surface being interrogated from the curvature values.

The optical interrogation means may alternatively comprise: a broadband optical source operable to generate a broad bandwidth optical signal having a spectral
25 bandwidth encompassing the spectral profile of an optical waveguide grating device to be interrogated, the optical source being optically coupled to one, input, end of the respective optical waveguide; and optical detection means optically coupled to the other, output, end of the optical waveguide, the optical detection means comprising an optical spectrum analyser operable to record the spectral profile of the optical waveguide grating device under interrogation and data processing means, such as a
30 microprocessor or personal computer, operable to match the recorded spectral profile with one of a plurality of pre-recorded spectral profiles, to thereby determine the curvature experienced by the grating device under interrogation.

The optical spectrum analyser and the data processing means are preferably portable.

30 According to a second aspect of the invention there is provided respiratory function monitoring apparatus comprising surface profiling apparatus according to the first aspect of the invention.

Preferably, the support structure of the coupling means comprises a garment of a size and shape suitable to closely fit across at least part of the thoracoabdominal surface of a subject whose respiratory function is to be monitored.

The data processing means is preferably operable to generate a 2- or 3- dimensional wire-frame image of the thoracoabdominal surface of a subject wearing the respiratory function monitoring apparatus, and is most preferably operable to repeatedly generate the image in real time, to thereby generate a changing, updating image of the thoracoabdominal surface.

Brief Description of the Drawings

Embodiments of the invention will now be described in detail, by way of example only, with reference to the accompanying drawings, in which:

Figure 1 is a schematic representation of shape profiling apparatus according to a first embodiment of the invention;

Figure 2 illustrates the effect on the transmission spectrum of a long period grating (period $480\mu\text{m}$) of the application of various curvatures $C\text{ m}^{-1}$) to the grating;

Figure 3 shows the attenuation profile of an optical waveguide grating device in the form of a long period grating for three different applied curvatures (C_1 , C_2 and C_3) together wavelength modulation range of a wavelength modulated narrow bandwidth optical signal;

Figure 4 shows a parametric plot of the first and second harmonics of the wavelength modulation frequency for various curvatures applied to a long period grating;

Figure 5 shows the arctan of the ratio (R) of the amplitudes of the first and second harmonics of the wavelength modulation frequency as a function of radius of curvature (C) for a long period grating of period $240\mu\text{m}$;

Figure 6 shows the arctan of the ratio (R) of the amplitudes of the first and second harmonics of the wavelength modulation frequency as a function of radius of curvature (C) for a long period grating of period $480\mu\text{m}$;

Figure 7 is a diagrammatic partially exploded plan view of a carrier member suitable for use with the apparatus of Fig.1;

Figure 8 is a diagrammatic sectional view along the line A-A of Fig.7;

Figure 9 shows the central wavelength of the attenuation band (4^{th} mode) of the third LPG 16 (period $350\mu\text{m}$) as a function of radius of curvature;

Figure 10 is a schematic representation of shape profiling apparatus according to a second embodiment of the invention;

Figure 11 is a schematic representation of shape profiling apparatus according to a third embodiment of the invention;

5 Figure 12 is a schematic representation of shape profiling apparatus according to a fourth embodiment of the invention

Figure 13 is a diagrammatic representation of respiratory function monitoring apparatus according to a fifth embodiment of the invention;

10 Figure 14 shows plots of percentage surface area error (E) as a function of number of monitoring locations for reconstructed CT scan chest profile data: (A) trapezoidal approximation; and (B) 4-point cubic spline interpolation;

Figure 15 is a diagrammatic representation of a torso showing the location of the carrier member on the upper chest (X) and the lower chest (Y);

15 Figure 16 shows the change in the central wavelength ($\Delta\lambda$) of the LPG's attenuation band as a function of the change in the circumference (Δc) of the torso, for the carrier member located on the lower chest (positions 2, 3 & 5); and

Figure 17 shows the change in the central wavelength ($\Delta\lambda$) of the LPG's attenuation band as a function of the change in the circumference (Δc) of the torso, for the carrier member located on the upper chest (positions 1 & 4).

20

Detailed Description

Referring to Figs. 1 to 9, a first embodiment of the invention provides surface profiling apparatus 10 utilising optical waveguide grating devices in the form of long period gratings (LPGs) 12, 14, 16 provided within respective sensing sections of single mode progressive three layered (PTL) optical fibre 18. Only three LPGs provided within a single carrier member are shown here for clarity but it will be appreciated that a larger number of LPGs may be used and may be provided within one or more carrier members.

30 LPGs consist of a periodic refractive index variation produced within the core of an optical fibre. The refractive index variation is induced within the fibre as a result of exposure of the fibre to ultra-violet radiation. The period of the refractive index variation is typically between 100 μ m and 600nm, and is much greater than the guided wavelength. An LPG acts to couple light incident on it from the fibre core into the fibre cladding, thereby producing attenuation bands within the transmission spectrum of the

optical fibre. Light is coupled from the core into the cladding with a spectral selectivity that is closely determined by the periodicity of the refractive index variation.

LPGs are sensitive to strain (ϵ), temperature (T) and the refractive index (n_s) of the surrounding medium. The sensitivity of an LPG to these parameters can manifest itself in two different ways: the central wavelength of the attenuation band can shift in wavelength; and a change in the spectral transmission profile of the attenuation band can occur. Of particular interest here is the sensitivity of LPGs to bending, which induces both a wavelength shift and a change in the spectral profile of the attenuation band.

The wavelength shift of the attenuation band arises as a result of the phase match condition of an LPG, which determines the spectral position of the attenuation band, and is given by

$$[n(co)_{eff}(\lambda, T, \epsilon) - n^v(cl)_{eff}(\lambda, T, n_s, \epsilon)] \cdot \Lambda(T, \epsilon) = \Delta n_{eff} \cdot \Lambda(T, \epsilon) = \lambda \quad (1)$$

15

where Λ is the period of the grating, $n(co)_{eff}$ is the effective refractive index of the core mode and $n^v(cl)_{eff}$ is the effective refractive index of the n^{th} radial cladding mode, both indices also being dependent on the refractive indices of the core and cladding, and on wavelength λ .

20

The magnitude of the wavelength shift induced by an applied strain, or a change in temperature or the refractive index of the surrounding medium, is dependent on the difference between the effective refractive indices of the core and the n^{th} radial cladding mode, and on the difference between the group effective refractive indices of the core and n^{th} radial cladding modes. The wavelength sensitivity of LPGs to bending arises from their sensitivity to strain. Bending an optical fibre induces strain and compression in the fibre, which in turn changes the group effective refractive indices of the core and the n^{th} radial cladding mode as well as $n(co)_{eff}$ and $n^v(cl)_{eff}$.

25

In the embodiment shown in Fig.1, the first LPG 12 has a period of 240 μ m, a length of 8cm and a strength of ~14dB, the second LPG 14 has a period of 480 μ m, a length of 10cm and a strength of ~10dB, and the third LPG 16 has a period of 350 μ m, a length of 10cm and a strength of ~10dB. The LPGs 12, 14, 16 were

30

fabricated using the point-to-point fabrication technique which will be well known to the skilled person and so will not be described in detail here. The PTL fibre used was not specifically designed to be photosensitive and so its photosensitivity was increased by hydrogenation at a pressure of 120 Bar for a period of 2 weeks at room temperature.

The periods of the LPGs 12, 14, 16 were chosen so that the associated cladding modes of the attenuation bands were from modes $n_{cl}(1,1)$ to $n_{cl}(1,10)$, which are known to be insensitive to the refractive index n_s of the surrounding medium.

The first LPG 12 produces an attenuation band having a central wavelength of ~1536nm, associated with its 9th cladding mode, the second LPG 14 produces an attenuation band having a central wavelength of ~1522nm, associated with its 5th cladding mode, and the third LPG 16 produces an attenuation band having a central wavelength of ~1520nm, associated with its 4th cladding mode.

Fig. 2 shows how the optical transmission spectrum (T) of the second LPG 14 changes as the radius of curvature applied to the LPG 14 is increased from 0 to 3.356m^{-1} .

In this example, the optical interrogation means takes the form of three distributed feedback (DFB) lasers 20, 22, 24 optically coupled to the input end 18a of the PTL fibre 18. The DFB lasers 20, 22, 24 are thermally stabilised and optical fibre pigtailed, and are operable to generate wavelength modulated, narrow bandwidth (i.e. narrow with respect to the spectral bandwidths of the LPGs 12, 14, 16 to be interrogated) optical signals. Both the wavelength of the optical signal generated by each DFB laser 20, 22, 24 and the frequency of the applied wavelength modulation are different for each DFB laser 20, 22, 24, and thus each respective LPG 12, 14, 16. The wavelength of each optical signal is selected to be close to the resonant wavelength of the respective LPG 12, 14, 16. The output fibre pigtails 20a, 22a, 24a of the DFB lasers 20, 22, 24 are optically coupled to the PTL fibre 18 via a 3x1 optical fibre multiplexer 36. A photodetector 26 is optically coupled to the output end 18b of the PTL fibre 18. The electrical output of the photodetector 26 is connected to three lock-in amplifiers 28, 30, 32. The different wavelength modulation frequencies are used to identify the LPG 12, 14, 16 which each part of the output signal generated by the photodetector 26 relates to, as will be described in more detail below.

The first DFB laser 20 generates a narrow bandwidth optical signal having a wavelength λ_1 of $\sim 1532\text{nm}$. An electrical sinusoidal modulation signal of a frequency ω_1 of 5kHz , generated by a signal generator 34, is applied to the laser injection current to thereby apply a sinusoidal wavelength modulation, having a first harmonic frequency of 5kHz and an amplitude of 0.06nm , to the optical signal. Modulating the wavelength at a particular modulation frequency ω_1 generates wavelength modulations on the optical signal at a series of harmonics of the modulation frequency i.e. $\omega_1, 2\omega_1$ etc. The second DFB laser 22 generates a narrow bandwidth optical signal having a wavelength λ_2 of $\sim 1517\text{nm}$. An electrical sinusoidal modulation signal of a frequency ω_2 of 3.7kHz , generated by the signal generator 34, is applied to the laser injection current to thereby produce a sinusoidal wavelength modulation having a first harmonic frequency of 3.7kHz and an amplitude of 0.06nm . The third DFB laser 24 generates a narrow bandwidth optical signal having a wavelength λ_3 of $\sim 1415\text{nm}$. An electrical sinusoidal modulation signal of a frequency ω_3 of 2.3kHz , generated by the signal generator 34, is applied to the laser injection current to thereby produce a sinusoidal wavelength modulation having a first harmonic frequency of 2.3kHz and an amplitude of 0.06nm . The drive current is set to operate in the saturation regimes of the DFB lasers 20, 22, 24 where the current induced amplitude modulation is minimised.

The series of wavelength modulation frequency harmonics present on each optical signal give rise to corresponding frequency components in the electrical output signal from the photodetector 26. The in-phase component of the n^{th} harmonic frequency component of the photodetector output signal is proportional to the n^{th} derivative of the spectral profile under interrogation. That is to say, the amplitudes of the first and second harmonic frequency components (ω_1 and $2\omega_1, \omega_2$ and $2\omega_2$, and ω_3 and $2\omega_3$) of the photodetector output signal are proportional to the first and second derivatives of the spectral transmission profiles of the respective LPGs 12, 14, 16.

Fig. 3 shows the attenuation profiles (percentage of transmission power (T) as a function of wavelength (λ)) of an LPG for three different curvatures (C_1, C_2 , and C_3), together with the wavelength modulation 38 at frequency ω of a DFB laser, which may be given by:

$$\lambda_{DFB} = \lambda_0 + \delta\lambda \sin(\omega t)$$

It can be seen in Fig.3 that the amplitude A_1 , A_2 , and A_3 of the photodetector output signal at frequency ω varies with the amount of curvature applied to the LPG.

In addition to the signals at modulation frequencies ω_1 , ω_2 and ω_3 , the signal generator 34 also generates sinusoidal electrical signals at the second harmonics of the modulation frequencies i.e. at $2\omega_1$, $2\omega_2$ and $2\omega_3$. The electrical signals generated by the signal generator 34 at frequencies ω_1 and $2\omega_1$ are passed to the first lock-in amplifier 28, the electrical signals at ω_2 and $2\omega_2$ are passed to the second lock-in amplifier 30, and the electrical signals at ω_3 and $2\omega_3$ are passed to the third lock-in amplifier 32. The lock-in amplifiers 28, 30, 32 are thereby set to measure the amplitudes of the first and second harmonic frequency components of the photodetector output signal corresponding to the first LPG 12, the second LPG 14 and the third LPG 16 respectively.

The ratio of the first and second derivatives is a unique function of position within the spectral transmission profile and is independent of any attenuation which may occur within the optical system. The amplitudes of the first and second harmonic frequency components can be represented by:

$$Amp^{1st} = A \sin(\xi) \quad \text{and} \quad Amp^{2nd} = B \sin(\xi + \alpha)$$

where ξ represents the degree of curvature experienced by an LPG under interrogation and α is the relative phase difference between the first and second harmonics. The ratio of the amplitudes of the harmonics is unique for a given radius of curvature, as illustrated in the parametric plot of the first and second harmonics recorded for radii of curvature of between 0 and 4.20m^{-1} shown in Fig. 4.

A more useful relationship between the amplitudes of the first and second harmonic frequency components of the photodetector output signal and the radius of curvature applied to an LPG is produced by taking the inverse tangent (arctan) of the ratio of the amplitudes of the first and second harmonics. This yields an approximately linear relationship between the arctan of the ratio of amplitudes and the radius of curvature, as shown in Figs. 5 and 6 for the first LPG 12 and the second LPG 14 respectively. A radius of curvature resolution of $\pm 0.05\text{m}^{-1}$ and a curvature measurement range of $\sim \pm 3\text{m}^{-1}$ is available in this example.

The spectral sensitivity $\frac{d\lambda}{dR}$ of the third LPG 16, i.e. the change in the central wavelength ($\Delta\lambda$) of the attenuation band associated with the fourth cladding mode, as a function of radius of curvature (R) is $3.747 \pm 0.002\text{nm.m}$, and is a linear relationship, as shown in Fig.9. The theoretically predicted wavelength shift is given by:

5

$$\Delta\lambda = \left[\frac{\Lambda\lambda}{(\delta n_{eff} - \delta n_g)} \cdot \frac{d\delta n_{eff}}{dR} + \frac{(\delta n_{eff})^3}{\delta n_g} \frac{d\Lambda}{dR} \right] \cdot \Delta R, \quad (2)$$

where $\delta n_{eff} = n_{coeff} - n_{cl_{eff}}$ is the differential effective index between the cladding

and the core mode and $\delta n_g = n_{cog} - n_{clg_v}$ is the differential group index. The

10 effective refractive indices of the core and 4th cladding mode are calculated as a function of curvature using a 2-D curvilinear hybrid mode eigenvalue equation. It is assumed that the amount of birefringence induced in a typical single mode fibre is negligibly small for curvatures of $< 2 \text{ m}^{-1}$, so no birefringence induced splitting of the attenuation band will occur. Fig. 9 demonstrates reasonable agreement
15 between the theoretical wavelength shift values 56 calculated at a number of different curvatures and the experimentally measured values 58.

In this embodiment the LPGs 12, 14, 16 are embedded within a carrier member 40, shown in Figs.1, 7 and 8. The carrier member 40 is deformable and takes the form of a skeleton 42 embedded between two sheets of flexible rubber skin 44, 46. The lower skin 46, which will be in contact with the surface to be
20 profiled, comprises a sheet (length 250mm, width 120mm and thickness 2mm) of natural latex rubber. This provides a flexible stage which is also thermally insulating. The upper skin 44 comprises a room temperature vulcanising clear silicon rubber ($n>1.5$), and has a thickness of approximately 3mm.

25 The skeleton 42 is partially rigid, but expandable, and is constructed from strips 50, 52, 54 (length 200mm, width 12mm, and thickness 0.254mm) of carbon steel, which support the sensing sections of the PTL fibre 18 containing the LPGs 12, 14, 16. The support strips 50, 52, 54 are fixed to the lower skin 46 and are arranged parallel to one another, approximately 75mm apart. Two connecting

strips 56 (length 80mm) are provided at either end of the support strips 50, 52, 54. V-section grooves 48 are formed along the length of the support strips 50, 52, 54 for receiving the sensing sections of the PTL fibre 18. The fibre is fixed to the support strips 50, 52, 54 using a cyanoacrylate adhesive. The v-grooves 48
 5 minimise bending of the LPGs 12, 14, 16 during the gluing process. The steel skeleton 42 gives longitudinal rigidity to the carrier member 40 and prevents the LPGs 12, 14, 16 from experiencing significant axial strain during use.

The steel skeleton also acts to stabilise the temperature of the LPGs 12, 14, 16. Over a 15°C temperature range the central wavelength of the attenuation
 10 mode associated with the 4th cladding mode of the third LPG 16 was observed to shift by 0.36nm. This gives a temperature sensitivity of

$$\frac{d\lambda}{dT} = 2.3 \pm 0.1 \times 10^{-2} \text{ nm}^\circ\text{C}^{-1}$$

15 Comparing this with a known temperature sensitivity of 0.198nm°C⁻¹ for the same cladding mode in bare PTL fibre, indicates that the temperature sensitivity of the LPGs 12, 14, 16 mounted on the carbon steel support strips 50, 52, 54 is approximately an order of magnitude smaller than that of bare PTL fibre. This reduction in temperature sensitivity of the LPGs 12, 14, 16 is due to the LPGs
 20 taking on the thermal expansion properties of the support strips.

In use, the carrier member 40 is placed on the surface to be profiled, with the lower skin 46 in contact with the surface. The radius of curvature of the surface at various monitoring locations is measured by the LPG provided at the respective monitoring location. The radius of curvature values measured by each
 25 LPG are input into a surface-modelling algorithm which creates a 2-dimensional or 3-dimensional wire-frame profile of the surface under investigation. By continually or repeatedly measuring the radius of curvature at each of the monitoring locations any changes in the profile of the surface can be monitored. Movement of the surface at one or more of the monitoring locations can also be tracked.

30 Surface profiling apparatus 60 according to a second embodiment of the invention is shown in Fig.10. The apparatus 60 is substantially the same as the surface profiling apparatus 10 of the first embodiment, with the following

modifications. The same reference numbers are retained for corresponding features.

In this embodiment the LPGs 12, 14, 16 are optically interrogated by wavelength modulated optical signals generated by illuminating three fibre Bragg gratings (FBGs) 62, 64, 66 with a broadband optical source in the form of a
 5 superluminescent light emitting diode (SLED) 68. The optical signal from the SLED 68 is routed to the FBGs 62, 64, 66 via an optical circulator (or coupler) 76. The light reflected by each of the FBGs 62, 64, 66 forms a narrow bandwidth optical signal which is coupled into the PTL fibre 18 through the circulator 76. Each
 10 optical signal has a central wavelength corresponding to the resonant wavelength of the respective FBG. Each FBG 62, 64, 66 has a different resonant wavelength, which lies within the spectral profile of its respective LPG 12, 14, 16. Each FBG 62, 64, 66 is coupled to tuning means in the form of a piezoelectric based strain apparatus 70, 72, 74 operable to apply an axial strain to the respective FBG 62,
 15 64, 66 at a desired modulation frequency. A wavelength modulation at that modulation frequency is thereby applied to the resonant wavelength of the FBG 62, 64, 66.

Similarly to the first embodiment, the modulation signals at frequencies ω_1 , ω_2 and ω_3 are generated by a signal generator 34. The modulation signals are
 20 applied to the drive voltage supplied from a drive unit 78 to the piezoelectric element in each strain apparatus 70, 72, 74. The piezoelectric element in each strain apparatus is thereby caused to expand and contract at the desired modulation frequency, so applying a varying axial strain to the respective FBG 62, 64, 66. A different modulation frequency is applied to each FBG.

Fig. 11 shows surface profiling apparatus 80 according to a third
 25 embodiment of the invention. The apparatus 80 is substantially the same as the surface profiling apparatus 10 of the first embodiment, with the following modifications. The same reference numbers are retained for corresponding features.

In this embodiment the LPGs 12, 14, 16 are optically interrogated by
 30 wavelength modulated optical signals generated by three FBG fibre lasers 82, 84, 86. The laser cavity of each fibre laser 82, 84, 86 is formed by two FBGs provided in a spaced relationship in a section of erbium-doped single mode optical fibre; the FBGs and the fibre forming the laser cavity. The fibre lasers 82, 84, 86 are

pumped by a 980nm pump laser 88, optically coupled to the erbium-doped fibre via an optical circulator (or coupler) 90.

Each fibre laser 82, 84, 86 lases at a wavelength determined by the resonant wavelength of its FBGs. Each pair of FBGs have a different resonant wavelength to thereby give each fibre laser 82, 84, 86 a different operating wavelength. The optical output signal from each fibre laser 82, 84, 86 is coupled to the PTL fibre 18 via the circulator 90. Each pair of FBGs is coupled to tuning means in the form of a piezoelectric based strain apparatus 92, 94, 96 operable to apply an axial strain to the FBGs at a desired modulation frequency, to thereby apply a wavelength modulation at that modulation frequency to the resonant wavelength of the FBGs. When the resonant wavelength of the FBGs in a fibre laser 82, 84, 86 changes, the operating wavelength of the fibre laser also changes. Therefore, applying an axial strain to the FBGs of a particular fibre laser 82, 84, 86 at a desired modulation frequency will apply a wavelength modulation at that frequency to the output wavelength of the fibre laser 82, 84, 86. A different modulation frequency is applied to each fibre laser.

As in the first embodiment, the modulation signals at frequencies ω_1 , ω_2 and ω_3 are generated by a signal generator 34. The modulation signals are applied to the drive voltage supplied from a drive unit 98 to the piezoelectric element in each strain apparatus 92, 94, 96. The piezoelectric element in each strain apparatus is thereby caused to expand and contract at the desired modulation frequency, so applying a varying axial strain to the FBGs of the respective fibre laser 82, 84, 86.

Surface profiling apparatus 120 according to a fourth embodiment of the invention is shown in Fig. 12. The apparatus 120 is similar to that shown in the first embodiment, but has different optical interrogation means 122, as described below. The same reference numbers are retained for corresponding features.

In this embodiment the LPGs 12, 14, 16 are illuminated by a broadband optical source in the form of a fibre pigtailed SLED 124, optically coupled to the input end 18a of the PTL fibre 18. The SLED 124 is operable to generate a broad bandwidth optical signal whose spectral range encompasses the spectral profiles of the attenuation bands of each of the LPGs 12, 14, 16. A small, portable optical spectrum analyser (OSA) 126, such as the "USB2000 Miniature Fiber Optic Spectrometer" from Oceanoptics Inc., is optically coupled to the output end 18b of

the PTL fibre 18. The OSA 126 is operable to record the spectral profiles of the attenuation bands of each of the LPGs 12, 14, 16. The OSA 126 is connected to a microprocessor 128, which may be a personal computer, to which the recorded spectral profile data is downloaded. The microprocessor 128 is operable to
5 compare the downloaded spectral profile data with a plurality of pre-recorded sets of spectral profile data, until a matching set of spectral profile data is found. Each set of pre-recorded spectral profile data corresponds to a particular curvature applied to a particular LPG, so a match indicates the curvature experienced by the LPG 12, 14, 16 under interrogation. The OSA 126 may be permanently connected
10 to the microprocessor 128, so that each recorded set of spectral profile data can be downloaded to, and processed by, the microprocessor 128 in real time. Alternatively, the OSA 126 does not have to be connected to the microprocessor 128 during interrogation of one or more LPGs 12, 14, 16. A number of spectral profiles may be recorded and stored in the OSA 126 for later downloading to, and
15 processing by, the microprocessor 128 once the OSA 126 is connected to it.

Referring to Figures 13 to 17, a fourth embodiment of the invention provides respiratory function monitoring apparatus 100 comprising surface profiling apparatus 102 which is substantially the same as the surface profiling apparatus 10, 60, 80, 120 according to one of the first, second, third or fourth embodiments,
20 with the following modifications. The same reference numbers as in the first embodiment are used for corresponding features (the first embodiment is selected for illustration only, and the skilled person will understand that the surface profiling apparatus according to the second, third or fourth embodiments may be used instead).

25 As shown in Fig. 13, in this example five LPGs (not shown) are provided within each of four carrier members 40a-d, giving a total of 20 LPGs. Each set of five LPGs are provided within a different PTL fibre 104, 106, 108, 110. There are four different optical arrangements which may be used to deal with this large number of LPGs. In the first, the attenuation band of each LPG has a different
30 central wavelength and the LPGs are interrogated by twenty wavelength modulated, narrow bandwidth optical signals generated by twenty DBF lasers (as in the first embodiment shown in Fig.1), by an SLED and twenty FBGs (as in the second embodiment shown in Fig.10), or by twenty fibre lasers (as in the third embodiment shown in Fig.11). The wavelength of each optical signal is different,

lying within the spectral bandwidth of the respective LPG, and each optical signal is wavelength modulated at a different modulation frequency. The output end of each PTL fibre 104, 106, 108, 110 is coupled to a single photodetector 26, and the electrical output signal from the photodetector is connected to twenty lock-in
5 amplifiers, each operating at the first and second harmonics of the modulation frequency of their respective optical signals.

In the second optical arrangement the attenuation band of each LPG again has a different central wavelength. The twenty LPGs are illuminated by a single broadband optical source, for example an SLED or an edge-emitting light emitting
10 diode (EELED). The spectral profiles of the attenuation bands are recorded by a single OSA and compared to pre-recorded spectral profiles using a microprocessor (as in the fourth embodiment shown in Fig.12).

In the third optical arrangement, each LPG within a set of five LPGs has a different attenuation band central wavelength, the LPGs in each of the four sets
15 having the same five central wavelengths. This means that only five narrow bandwidth optical signals, having five different wavelengths, are required to interrogate all twenty LPGs, since each optical signal can be used to interrogate four separate LPGs. By connecting the output end of each PTL fibre 104, 106, 108, 110 to a different photodetector, only five different wavelength modulation
20 frequencies are required. The photodetectors thereby identify which carrier member 40a-d a signal relates to, and the modulation frequency identifies the LPG within that carrier member 40a-d, thereby identifying the respective monitoring location.

The fourth optical arrangement similarly uses four sets of five LPGs. In this
25 case all of the LPGs can be illuminated using a single broadband optical source, SLED or EELED. The output end of each PTL fibre 104, 106, 108, 110 is connected to a different OSA, since the LPGs within each set are identified by wavelength. The spectral profiles recorded by the OSAs can be downloaded to a single microprocessor for processing to determine the curvature experience by
30 each LPG, as in the fourth embodiment.

In this embodiment the respiratory function monitoring apparatus 100 is intended for use on a human subject and the curvature values are used to generate a 3-dimensional wire-frame image of the thoracoabdominal surface. Testing of the apparatus 100 was carried out on a commercial resuscitation training

aid manikin. The manikin comprises a rigid under-frame over which a polymer skin is stretched. An inflatable air bag is provided between the frame and skin, and can be inflated and deflated to simulate expansion and contraction of the surface of the torso in similar volumetric proportions to that of breathing.

5 The number of LPGs required to monitor the respiratory function of an adult human subject was determined using chest profile data obtained from a CT imager. The upper chest geometry of a male subject was reconstructed using a 7th order polynomial and the surface area evaluated. This was then compared to the area estimated using simple trapezoidal and four-point cubic-spline integrations at lower
10 sampling resolutions in order to obtain an estimate of the error dependence on the number of monitoring locations, i.e. the number of LPGs, within the surface profiling apparatus 102.

 Fig. 14 shows a plot (A) of surface area error (calculated using the trapezoidal integration) as a function of the number of monitoring locations/LPGs
15 provided across a torso (assuming that the same resolution is required longitudinally and laterally). The second plot (B) shows surface area error (calculated using the cubic-spline interpolation) as a function of number of LPGs. Considering these values together with generally accepted volumetric performance
20 standards for spirometry based respiratory function monitoring devices, confirms that the respiratory function monitoring apparatus 100 requires in the region of 20 LPGs (using cubic-spline interpolation) to provide a similar performance.

 The response of one LPG within one carrier member 40 was investigated, using an OSA, at various degrees of inflation of the manikin, at five different
25 locations on the manikin. Each location is represented by a set of dimensions given in the following table, and shown in Fig.15.

5	Position on torso Fig. 15 (X)	d ₁ (mm)	d ₂ (mm)	d ₃ (mm)	d ₄ (mm)	Maximum detected wavelength shift (nm)
	1	90	50	50	250	1.05
	2	185	50	50	185	3.18
	3	287	50	50	75	0.95
10	Position on torso Fig. 15 (Y)	p ₁ (mm)	p ₂ (mm)	p ₃ (mm)	p ₄ (mm)	Maximum detected wavelength shift (nm)
	4	205	25	165	165	1.98
	5	100	128	165	165	1.70
15						
20						

The change in the central wavelength of the LPG's attenuation band as a function of the peripheral expansion of the manikin's skin (change in the circumference of the manikin's torso) was also investigated, shown in Figs. 16 and 17. The variation in response of the LPG apparent between locations on the upper and lower chest regions mimics that which might be expected in a real human subject, as the expansion of the rib cage has a more significant contribution at higher levels of ventilation.

Figs. 16 and 17 show that the spectral response of the LPG as a function of peripheral expansion of the manikin's skin varies with location on the torso. The errors shown in these figures correspond to the spectral accuracy ($\pm 0.04\text{nm}$) of the OSA used to measure the change in wavelength and a torso circumference error of $\pm 1\text{cm}$. The circumference error is an estimate of the variation of the manikin's skin deformation between each set of results.

As discussed above in connection with the first embodiment, LPGs are temperature sensitive, although this has been reduced by an order of magnitude due to the fact that the LPGs 12, 14, 16 are fixed to steel support strips 50, 52, 54.

The temperature sensitivity of the LPGs will introduce an error into the measurement process during monitoring of respiratory function, since the surface profiling apparatus 10, 60, 80 is intended to be used in close contact with the skin. Assuming a typical skin temperature variation of $\sim 32^{\circ}\text{C}$ to $\sim 35^{\circ}\text{C}$ this would generate a maximum wavelength error of $\pm 0.035\text{ nm}$. Using the maximum detected wavelength shift presented in the above table, this gives a maximum (worst case) relative error of $\sim \pm 3\%$ (position 3) and a minimum relative error of $\sim \pm 1\%$ (position 2).

As shown in Fig.13 the carrier members 40a-d are attached to a garment 114 which is worn by the subject. The garment 114 shown is illustrative only and would in practice be of a closer fit to the subject's skin, so that the carrier members 40a-d are in close contact with the skin. Providing the carrier members 40a-d on a garment 114 assists in the correct positioning of the LPGs across the surface to be profiled, i.e. the torso. The optical interrogation means 112 in this example is carried by a belt 116 worn around the subject's waist, but it could alternatively be attached to the garment 114, or be provided with attachment means, such as a mechanical clip or fleece and hook fastener, by which the subject may attach the optical interrogation means 112 to an item of clothing.

The surface profiling apparatus of the described embodiments provide the advantage of having a curvature spectral sensitivity of 3.747 nm.m and the temperature sensitivity of the LPGs is reduced by approximately an order of magnitude by mounting them on carbon steel support strips. The LPGs display negligible axial strain due to their being fixed to the support strips. The surface profiling apparatus can be used to distinguish between various geometric variations associated with different locations on a moving surface, including a human torso during respiratory movement. The fabrication of the LPGs in a multi-clad single mode optical fibre, such as PTL, makes the LPGs insensitive to the refractive index of a surrounding medium. Each of the described optical interrogation apparatus is portable, enabling the profile of a surface to be monitored in a real situation (i.e. outside of a laboratory environment) and allows the subject on which the surface is located to move freely during measurement and monitoring.

The surface profiling apparatus does not need to be calibrated for each surface under investigation. The optical grating sensors (LPGs) only need to be

calibrated once: change in the electrical output signal as a function of change in curvature experienced by an LPG.

5 The respiratory function monitoring apparatus described provides monitoring apparatus which can assess lung function without the need for flow measurement at the mouth. The apparatus can also provide detailed information of the dynamics of chest motion during breathing. The described apparatus will facilitate further studies of respiratory physiology, because unlike previously known systems, it can provide a completely non-invasive and quantitative appreciation of respiratory function. Using 20 LPG sensors allows the apparatus to be used to
10 generate a geometrical profile of the chest and abdomen in three dimensions with the necessary accuracy. The apparatus provides a curvature resolution of $\pm 2.0 \times 10^{-2} \text{ m}^{-1}$ which is a relative error of $\pm 1\%$ over the curvature measurement range of the apparatus.

15 The respiratory function monitoring apparatus described re-approaches the less complex, useful two compartment monitoring technology from a geometrical aspect with a view to enhancing the performance and adding functionality. The apparatus enables a 3-dimensional profile of the thoracoabdominal surface to be generated, using an on-body reference. The apparatus enables the movement of selected anatomical positions on the chest and abdomen surface to be tracked
20 during breathing manoeuvres, as well as facilitating measurements of tidal respiratory volume. The curvature values generated by the apparatus are input into a surface-modelling algorithm to create a 2- or 3-dimensional wire-frame image of the thoracoabdominal surface.

25 The electronic and optical elements of the optical interrogation means can be made very small and therefore portable. This means that the respiratory function monitoring apparatus can be attached to the subject, enabling the subject to move freely without constraint whilst their breathing is monitored. The apparatus thereby provides an improved diagnostic tool for continuous monitoring of patients in a healthcare environment.

30 Various modifications may be made without departing from the scope of the invention. Referring to the surface profiling apparatus itself, a different type of optical fibre may be used to that described, including multilayer optical fibres having three or more cladding layers. The structure of the optical fibre may be asymmetrical about its axis. The LPGs may include sections in which the grating

period is chirped, or may include one or more phase-shifts within the periodic refractive index modulation, to provide additional information about the direction of the curvature. The LPGs may alternatively or additionally be asymmetric about the axis of the fibre. The LPGs may be replaced by an alternative optical waveguide grating curvature sensing device, such as two long period gratings arranged to
5 together define an in-line Mach-Zehnder interferometer, an optical waveguide Bragg grating, or two optical waveguide Bragg gratings arranged to together define a Fabry-Perot etalon.

The coupling means may comprise a different number of carrier members to that described, and a different number of optical waveguide grating curvature sensing devices may be provided within each carrier member. In particular, a single carrier member, of a size and shape suitable to provide a close fit to the surface to be profiled, may be used. The arrangement of the LPGs within a carrier member may be different to that used. The carrier member may have a different
15 structure to that described, in particular a skeleton may not be necessary for mechanically strong types of optical fibre, such as polymer fibre. The skin of the carrier member may comprise a different flexible material.

In the case of an inanimate subject a carrier member may not be required, the optical waveguide grating curvature sensing devices being attached directly to,
20 or embedded within, the surface to be profiled.

The optical interrogation means may utilise different optical sources operable to generate a wavelength modulated, narrow bandwidth optical signal. Also, different optical detection means may be used to that described. In particular, a different number of photodetectors may be used and the lock-in
25 amplifiers may be replaced by a different type of synchronous detector. A different optical spectrum analyser to that described may be used in connection with the surface profiling apparatus of the described fourth embodiment.

Referring in particular to the respiratory function monitoring apparatus, a different number of carrier members may be used, and each carrier member may
30 incorporate a different number of LPGs. The garment incorporating the carrier members may be different to that described.

CLAIMS

1. Surface profiling apparatus characterised by comprising:
an optical waveguide including a plurality of sensor sections in which a
5 plurality of optical waveguide grating curvature sensing devices are respectively
provided; and
optical interrogation means operable to interrogate the optical waveguide
grating curvature sensing devices, to determine the curvature experienced by each
device,
10 whereby a profile of a surface to which the sensor sections of the optical
waveguide are coupled may be constructed from the curvatures sensed by the
optical waveguide grating curvature sensing devices.
2. Apparatus as claimed in claim 1, wherein the optical waveguide is an optical
15 fibre, such as a silica-glass optical fibre or a polymer optical fibre, the optical fibre
comprising a core, an inner cladding layer surrounding the core, and at least a first
outer cladding layer surrounding the inner cladding layer, the refractive index of the
inner cladding layer being less than the refractive index of the core, and the
refractive index of the first outer cladding layer being less than the refractive index
20 of the inner cladding layer.
3. Apparatus as claimed in claim 2, wherein the optical fibre further comprises
a second outer cladding layer surrounding the first outer cladding layer in order to
isolate light propagating within a cladding mode of the inner cladding layer from a
25 medium surrounding the outermost cladding layer, the refractive index of the
second outer cladding layer being less than the refractive index of the first outer
cladding layer.
4. Apparatus as claimed in any preceding claim, wherein an optical waveguide
30 grating curvature sensing device comprises an optical waveguide grating device,
such as long period grating, two long period gratings arranged to together define
an in-line Mach-Zehnder interferometer, an optical waveguide Bragg grating, or two
optical waveguide Bragg gratings arranged to together define a Fabry-Perot etalon.

5. Apparatus as claimed in any preceding claim, wherein the surface profiling apparatus further comprises coupling means for coupling the sensor sections of the optical waveguide to the surface to be profiled, the coupling means comprising a carrier member, and the sensor sections of the optical waveguide being fixed to or embedded within the carrier member.

6. Apparatus as claimed in claim 5, wherein the coupling means comprises a plurality of carrier members mounted on a support structure, one or more optical waveguide sensor sections being fixed to or embedded within each carrier member.

7. Apparatus as claimed in claims 5 or 6, wherein the or each carrier member is deformable and comprises a flexible skin fixed to a partially rigid, expandable skeleton structure.

8. Apparatus as claimed in any preceding claim, wherein the optical interrogation means is a derivative spectroscopy or synthetic heterodyne based optical interrogation means operable to detect changes in the spectral profile of an optical waveguide grating device, the optical interrogation means comprising:
an optical source operable to generate a narrow spectral bandwidth wavelength modulated optical signal at a wavelength within the spectral range of an optical waveguide grating device to be interrogated, the optical source being optically coupled to one, input, end of the respective optical waveguide; and
optical detection means optically coupled to the other, output, end of the optical waveguide and being operable to detect changes in the spectral transmission profile of the optical waveguide grating device being interrogated and to thereby determine the curvature experienced by the grating device.

9. Apparatus as claimed in claim 8, wherein the optical detection means comprises:

a photodetector optically coupled to the output end of the or each optical waveguide and a plurality, corresponding to the number of optical waveguide grating devices provided within the respective waveguide, of lock-in amplifiers or synchronous detectors each operable to measure the amplitude of a detected

optical signal at the modulation frequency associated with a particular optical waveguide grating device and a harmonic of the modulation frequency; and

5 data processing means connected to the or each photodetector, operable to calculate the ratio of the amplitudes and the arc tangent of the ratio of the amplitudes, to which the curvature experienced by the optical waveguide grating device under interrogation is linearly related.

10. Apparatus as claimed in any of claims 1 to 7, wherein the optical interrogation means comprises:

10 a broadband optical source operable to generate a broad bandwidth optical signal having a spectral bandwidth encompassing the spectral profile of an optical waveguide grating device to be interrogated, the optical source being optically coupled to one, input, end of the respective optical waveguide; and

15 optical detection means optically coupled to the other, output, end of the optical waveguide, the optical detection means comprising an optical spectrum analyser operable to record the spectral profile of the optical waveguide grating device under interrogation and data processing means operable to match the recorded spectral profile with one of a plurality of pre-recorded spectral profiles, to thereby determine the curvature experienced by the grating device under
20 interrogation.

11. Respiratory function monitoring apparatus comprising surface profiling apparatus as claimed in any preceding claim.

ABSTRACT
SURFACE PROFILING APPARATUS

5 Surface profiling apparatus 10 according to one embodiment comprises
three long period gratings (LPGs) 12, 14, 16 fabricated in progressive three layered
(PTL) fibre 18 and embedded within a deformable carrier member 40 comprising a
skeleton 42 provided between two sheets of flexible rubber skin 44, 46. The LPGs
12, 14, 16 are illuminated by three wavelength modulated, narrow bandwidth
10 optical signals, each having a different wavelength and modulation frequency. A
photodetector 26 connected to three lock-in amplifiers 28, 30, 32 measures the
amplitudes of the first and second harmonic frequency components of the
photodetector output signal corresponding to each LPG 12, 14, 16. Similar surface
profiling apparatus 10 forms the basis for respiratory function monitoring apparatus
15 100 in which five LPGs are provided within each of four PTL fibres 104, 106, 108,
110, and embedded in four carrier members 40a-d attached to a garment 114 to be
worn by a subject.

(Fig. 1)

20

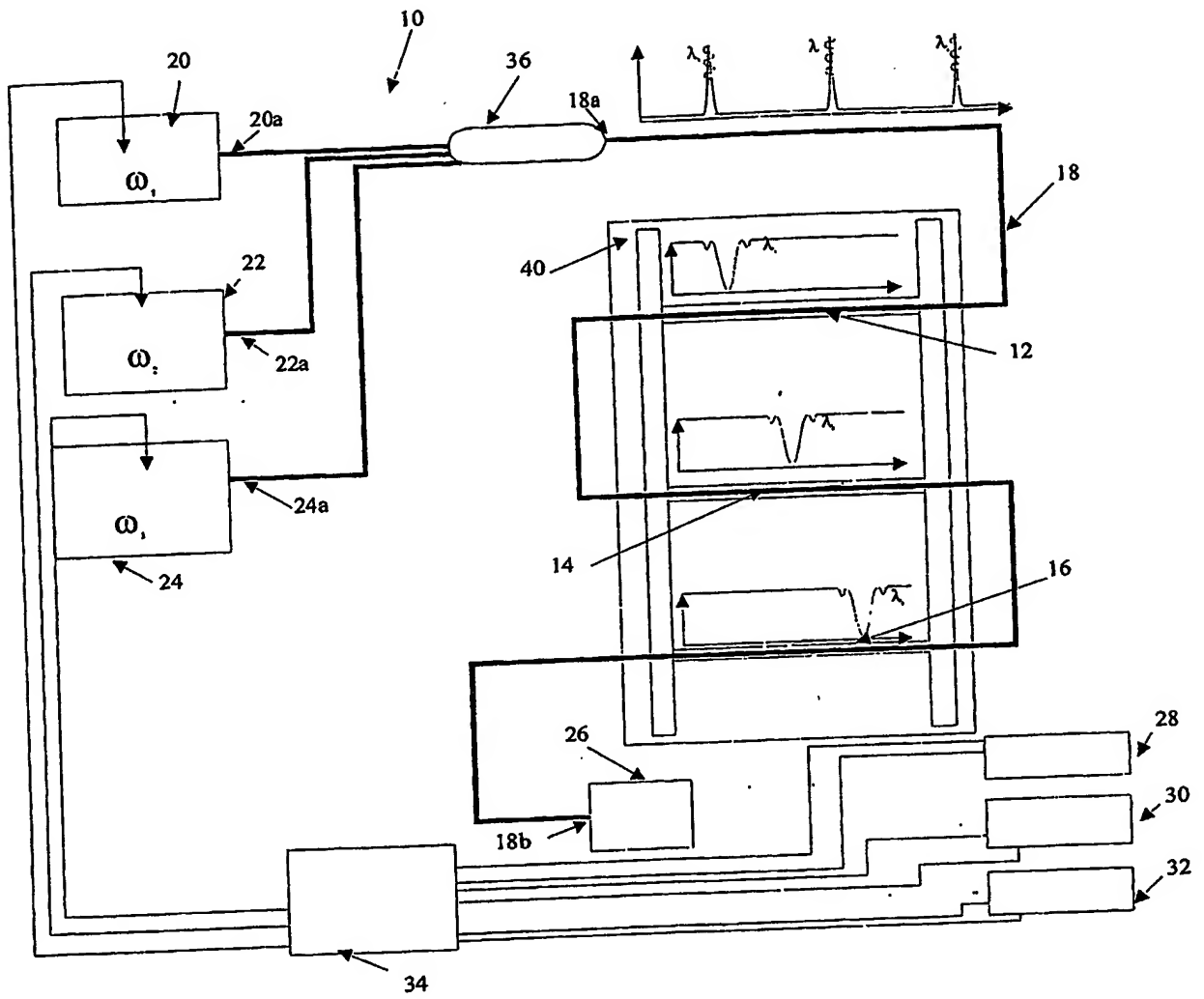


Figure 1

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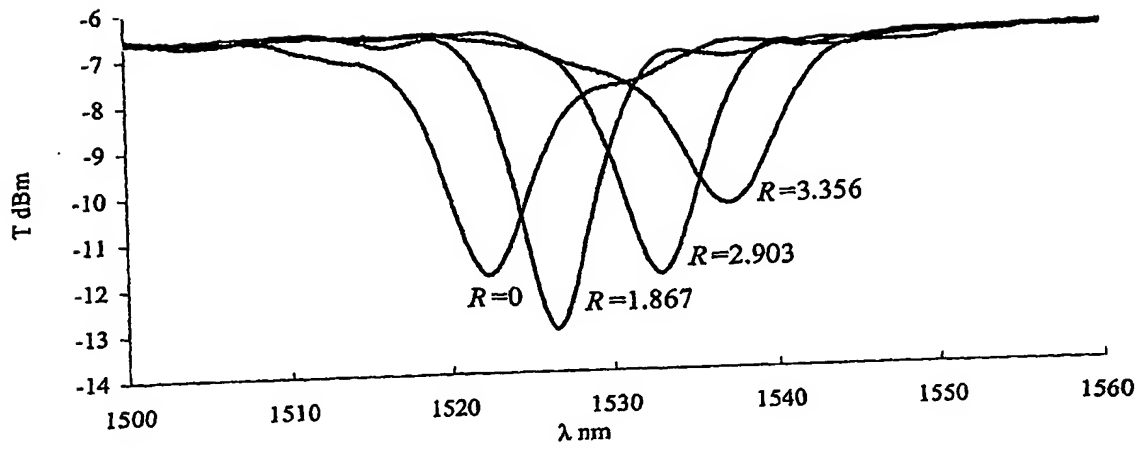


Figure 2

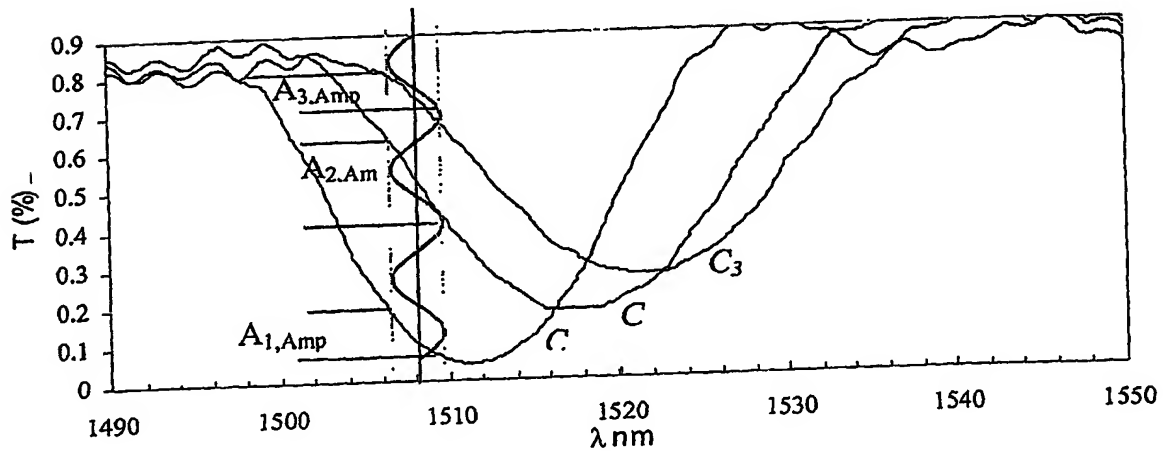


Figure 3

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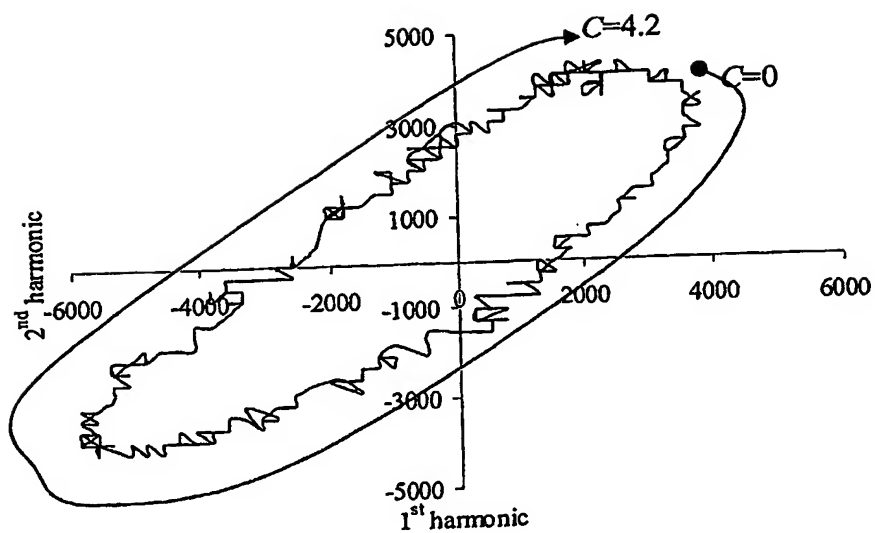


Figure 4

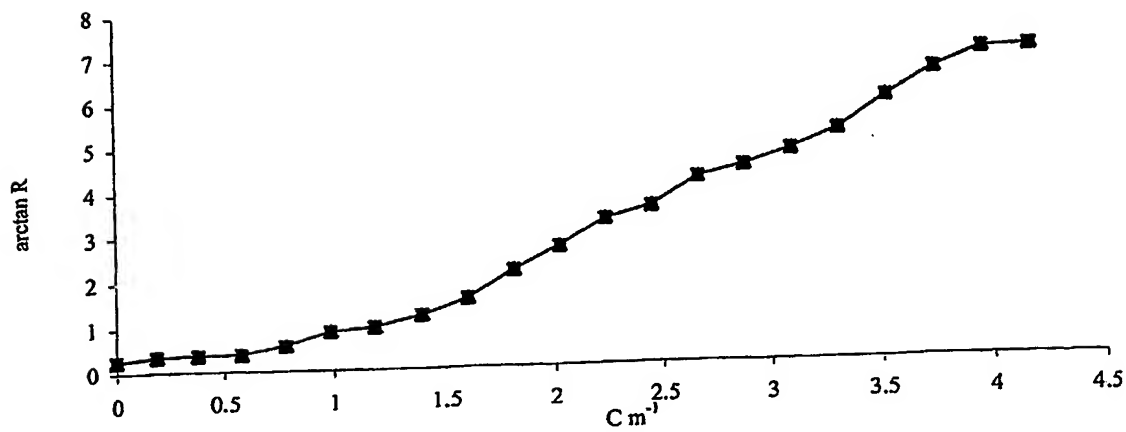


Figure 5

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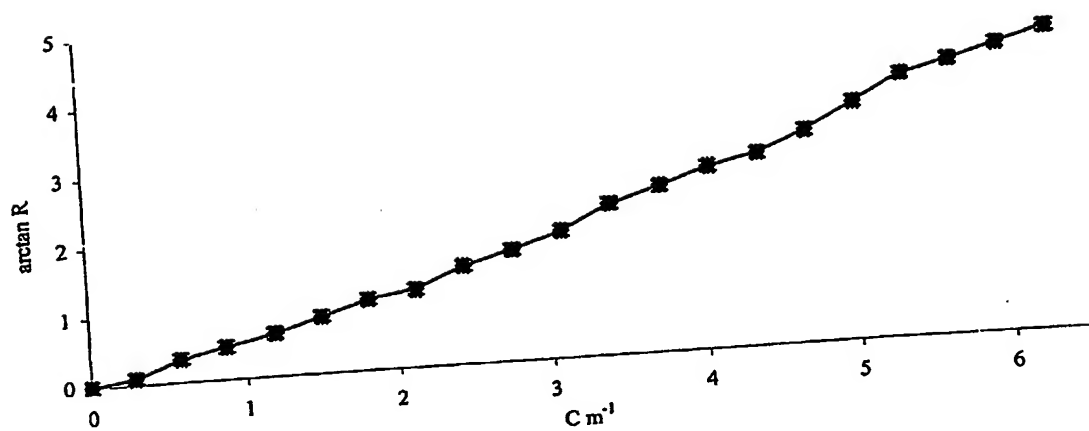


Figure 6

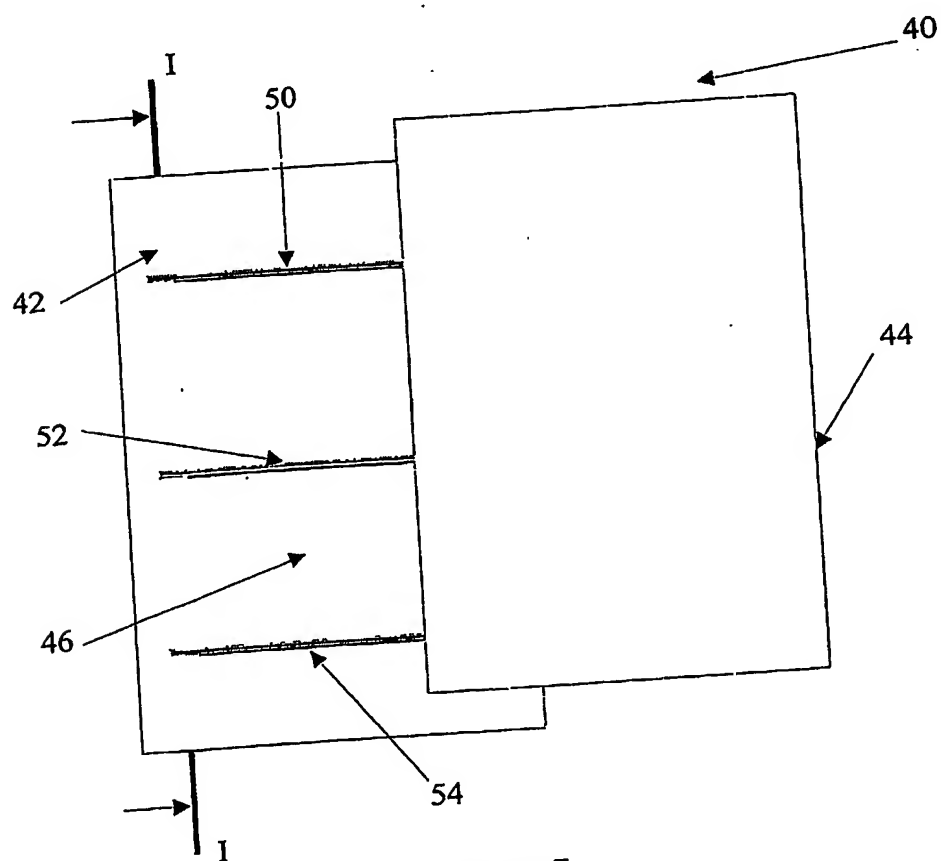


Figure 7

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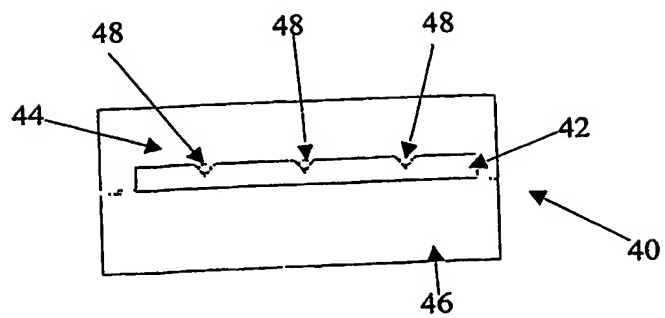


Figure 8

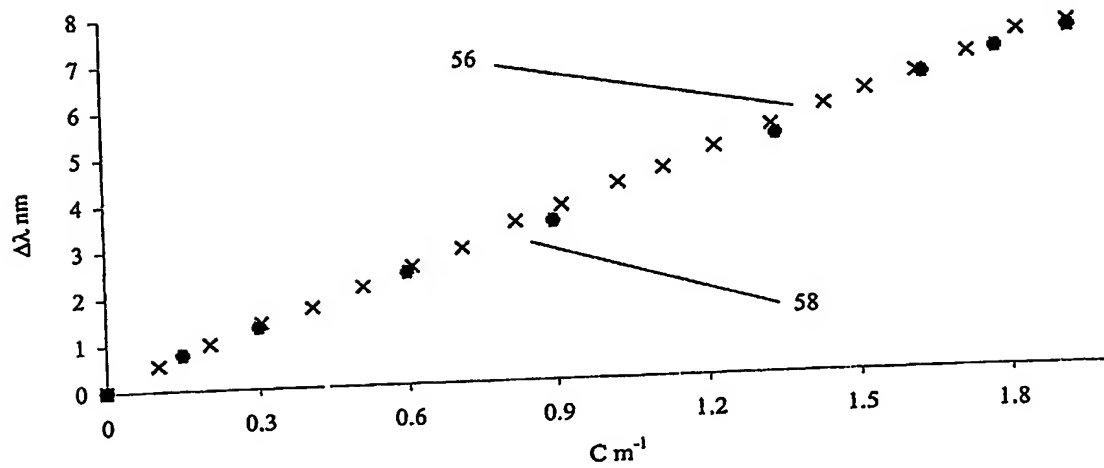


Figure 9

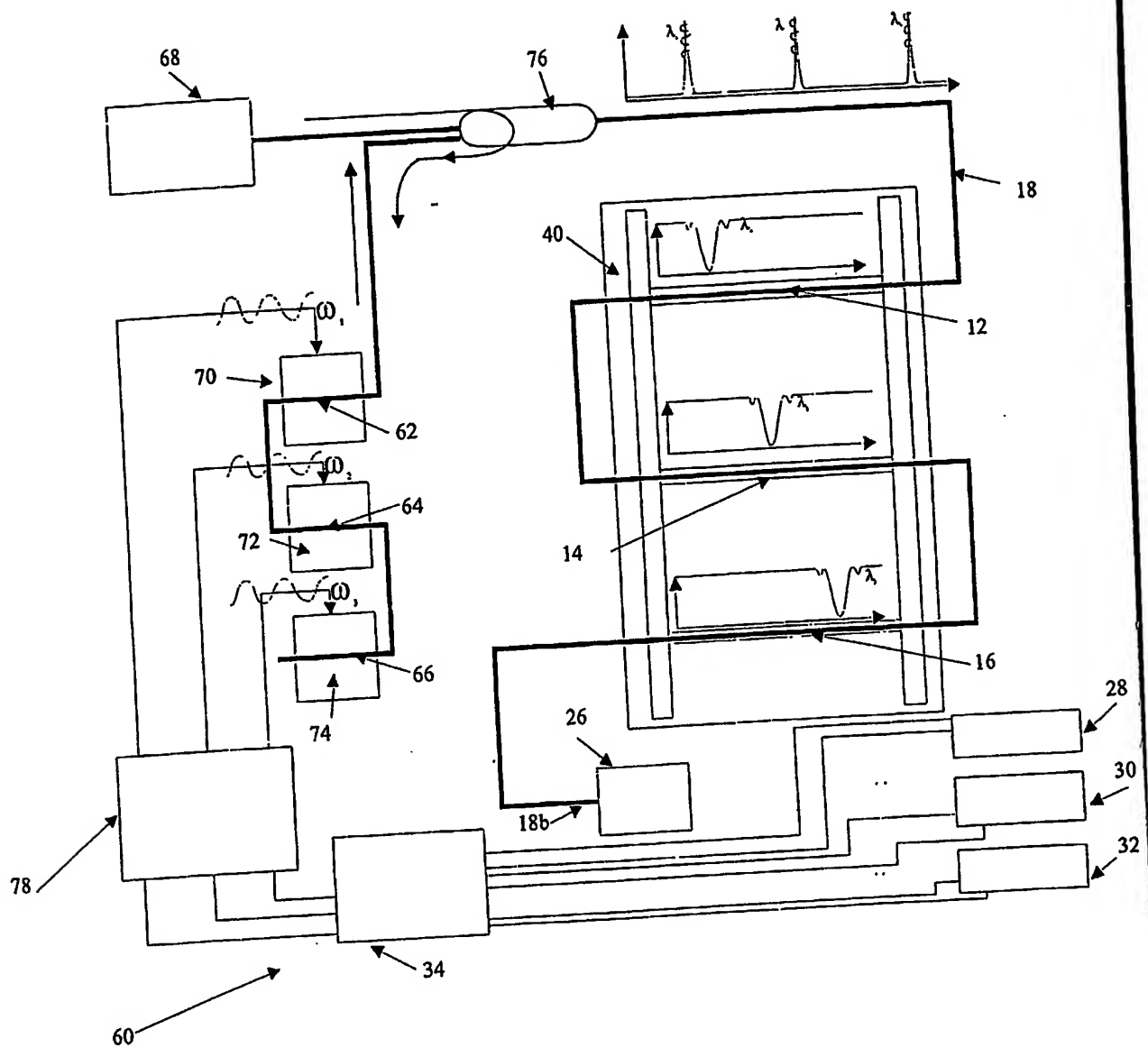


Figure 10

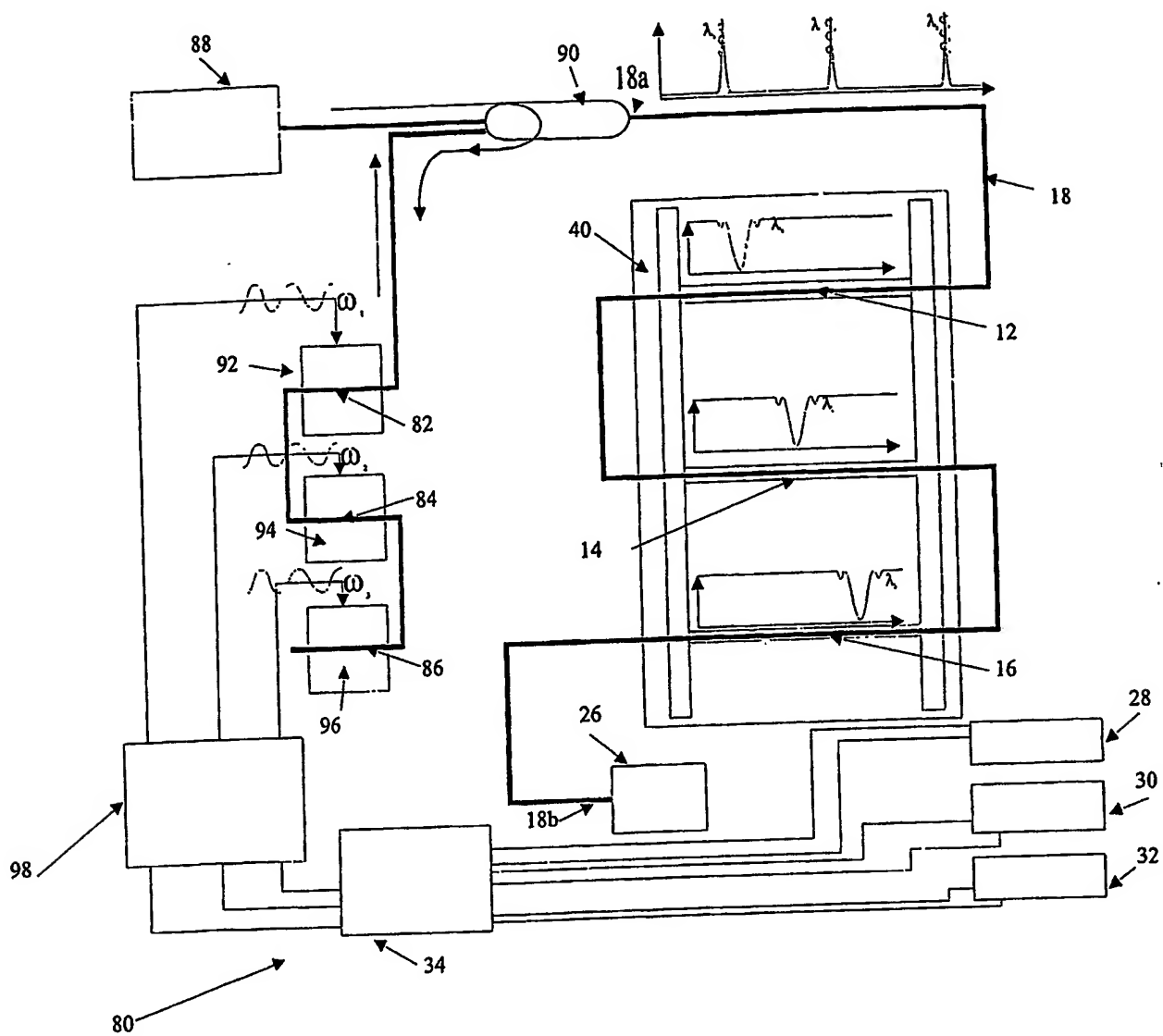


Figure 11

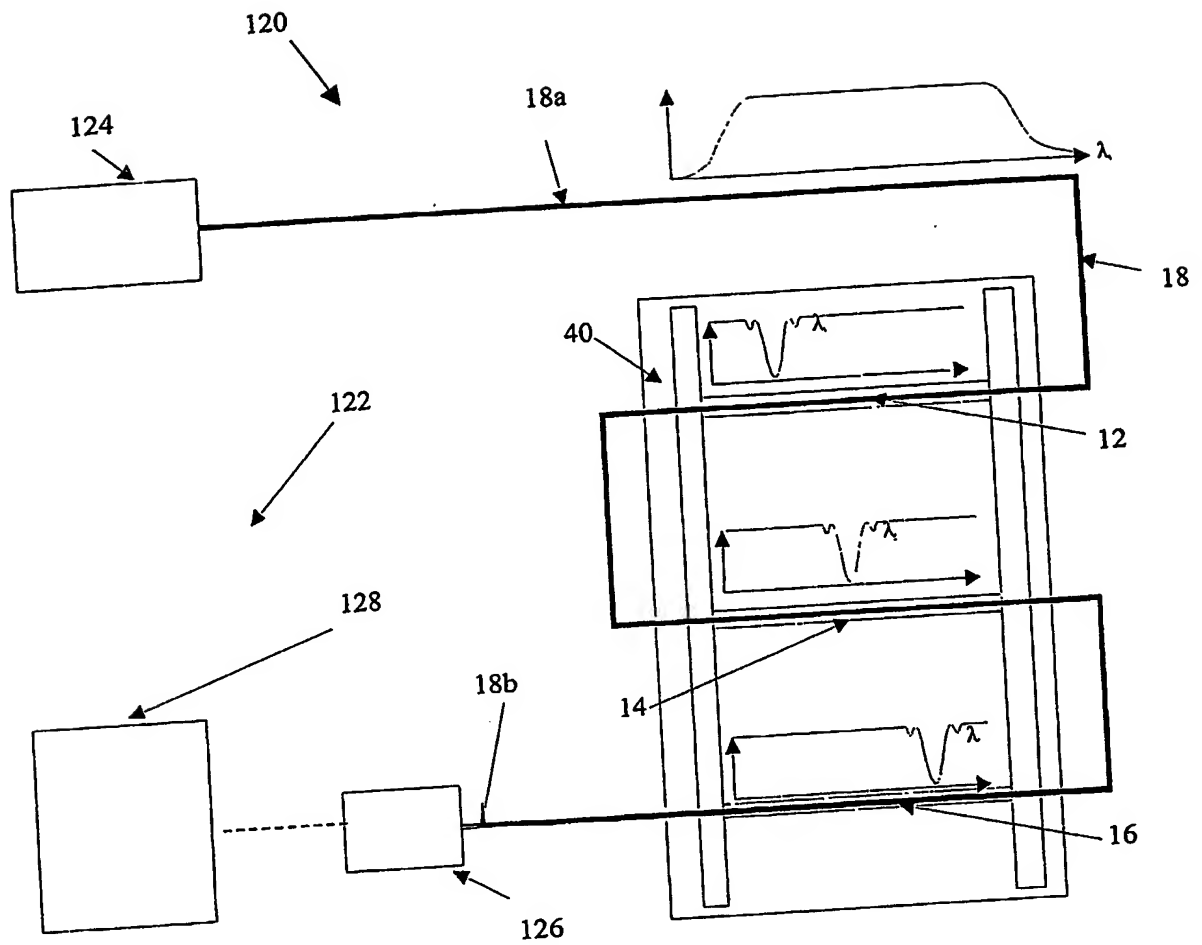


Figure 12

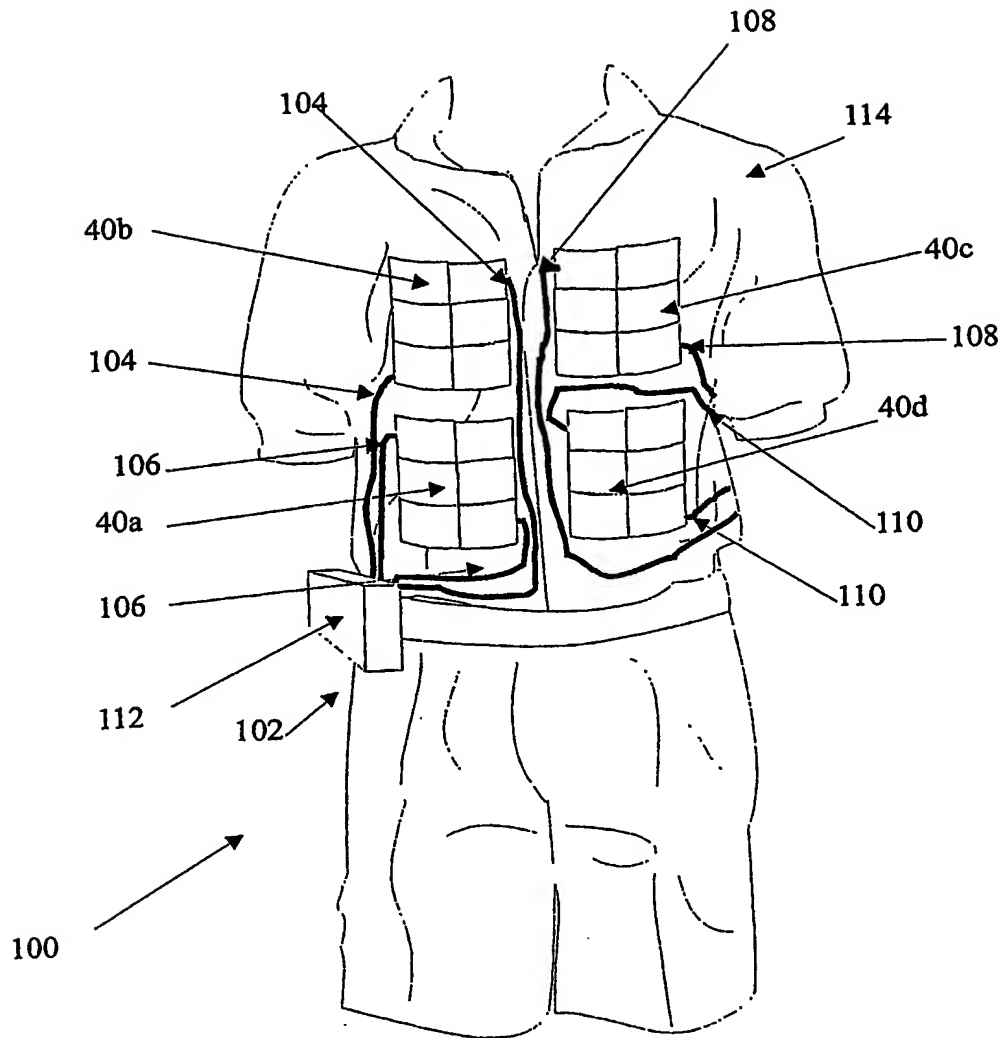


Figure 13

10/12

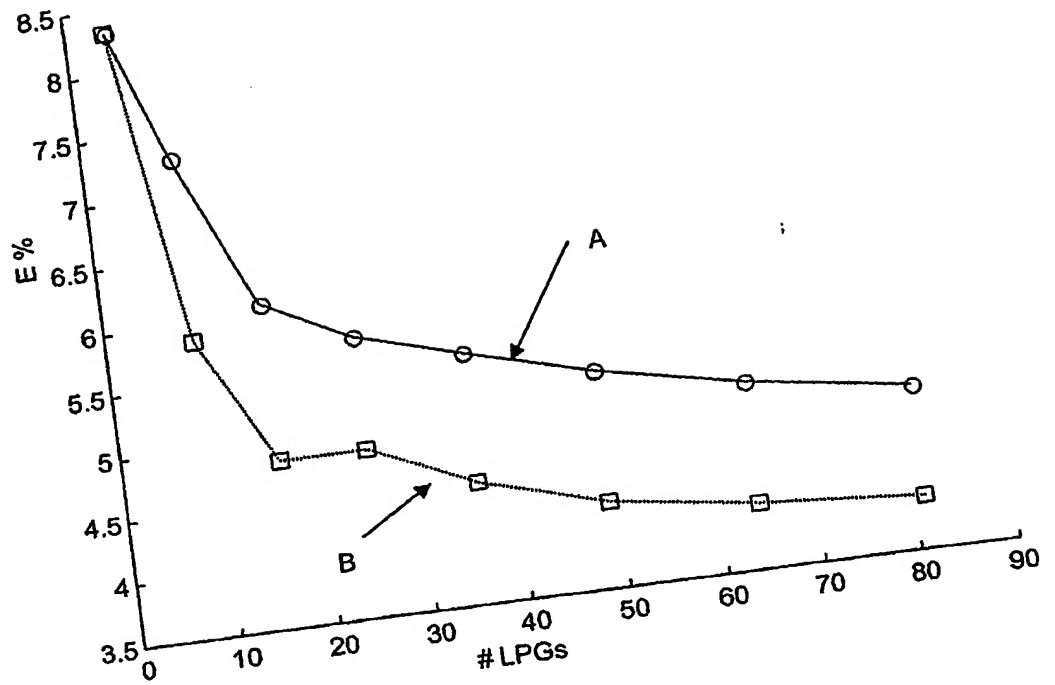


Figure 14

11/12

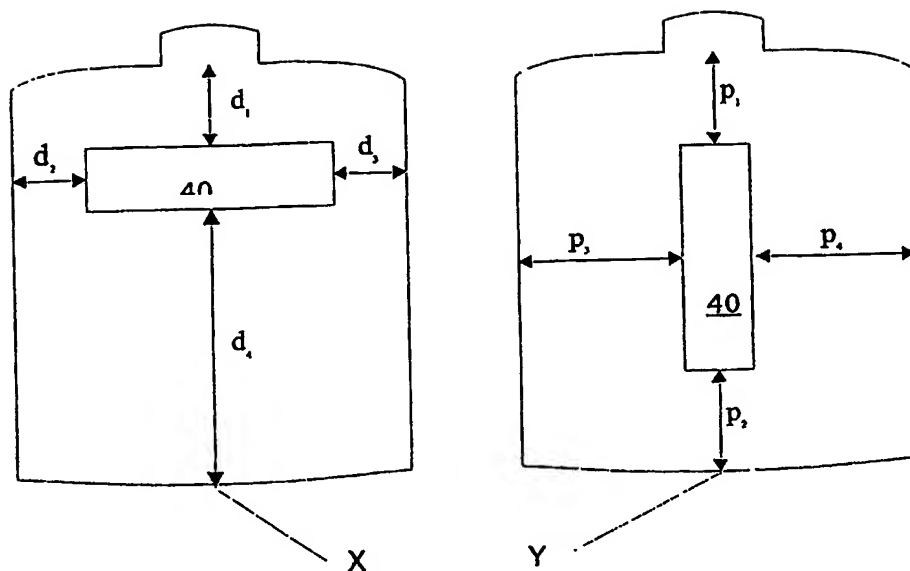


Figure 15

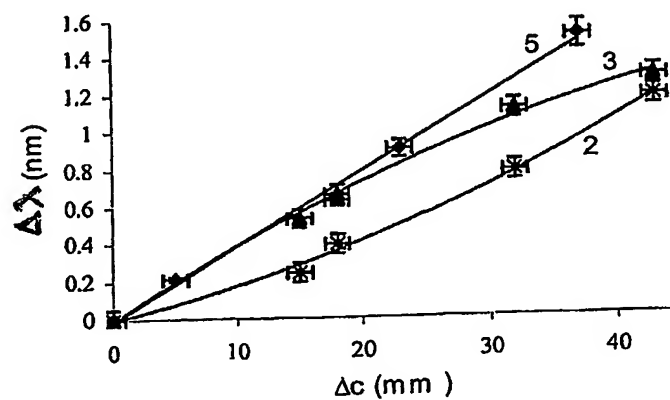


Figure 16

12/12

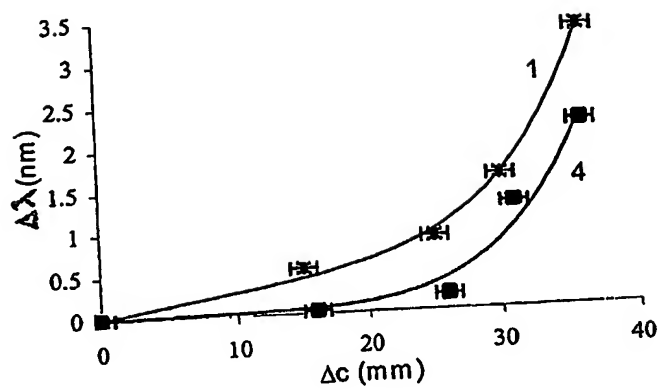


Figure 17

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